

Robust Pictorial Structures for X-ray Animal Skeleton Tracking

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Abstract: The detailed understanding of animals in locomotion is a relevant field of research in biology, biomechanics and robotics. To examine the locomotor system of birds *in vivo* and in a surgically non-invasive manner, high-speed X-ray acquisition is the state of the art. For a biological evaluation, it is crucial to locate relevant anatomical structures of the locomotor system. There is an urgent need for automating this task, as vast amounts of data exist and a manual annotation is extremely time-consuming. We present a biologically motivated skeleton model tracking framework based on a pictorial structure approach which is extended by robust sub-template matching. This combination makes it possible to deal with severe self-occlusions and challenging ambiguities. As opposed to model-driven methods which require a substantial amount of labeled training samples, our approach is entirely data-driven and can easily handle unseen cases. Thus, it is well suited for large scale biological applications at a minimum of manual interaction. We validate the performance of our approach based on 24 real-world X-ray locomotion datasets, and achieve results which are comparable to established methods while clearly outperforming more general approaches.

1 INTRODUCTION

The in-depth understanding of animal locomotion is an ongoing field of research with relevant applications in biology (Fischer and Lilje, 2011; Stoessel and Fischer, 2012), biomechanics (Brainerd et al., 2010; Nyakatura et al., 2012), and robotics, and includes the development of mathematical models for locomotion, obtaining a detailed understanding of evolution or developing walking robots. Especially avian bipedal locomotion represents a suitable testbed for detailed studies due to the large variety of existing species with different properties such as body size, mass, limb proportions, as well as walking speed and behavior. To examine the locomotor system of birds *in vivo* and in a surgically non-invasive manner, high-speed X-ray acquisition is the state of the art. As the animal to be analyzed is usually placed on a treadmill, X-ray videography provides an unbiased and highly detailed insight into locomotion characteristics. A typical X-ray recording setup and the resulting data is exemplarily shown in Fig. 1 and described in detail in (Stoessel and Fischer, 2012). To allow for highly accurate studies and analyses, recordings are generally performed at a high spatial and temporal resolution—in our case 1536×1024 pixels at a frame rate of 1 kHz.

This huge amount of data, on the other hand, has a big drawback at the same time, as the biological eval-

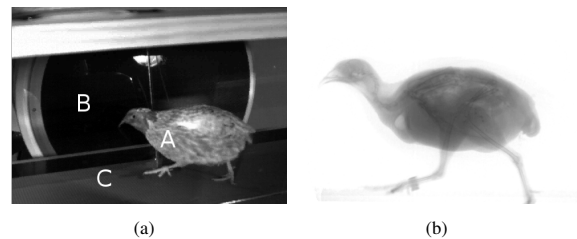


Figure 1: (a) X-ray recording procedure during locomotion showing a quail (A) on a treadmill (C) within the X-ray acquisition system (B). The corresponding acquired data frame is shown in (b).

uation heavily relies on finding anatomical landmarks such as hip joints, knee joints, or the feet in each frame of a recorded sequence. Until today, the automated localization of those landmarks is still in its infancy and often has to be performed by human experts, as self-occlusions of the locomotor system drastically complicate this task. In (Gatesy et al., 2010), for instance, a 3D skeleton model is fitted manually to X-ray scans of animals. However, for biological and biomechanical purposes, large-scale studies including thousands of sequences are highly desirable but are only feasible if a time-consuming manual interaction is avoided.

In this paper, our goal is to overcome limitations of recent approaches for X-ray tracking in animal locomotion scenarios. In particular, our focus is to pro-

vide a novel data-driven tracking approach which uses global information while being robust to local occlusions and does not rely on any training data. Thus, a fully automated application to large amounts of data is possible at a minimum of user interaction.

In Sect. 2, we give an overview of related work and motivate our approach. Sect. 3 briefly presents the methods which form the basis for our extended tracking method, while our proposed robust tracking approach is discussed in Sect. 4. The evaluation of our approach on real-world datasets is given Sect. 5.

2 RELATED WORK AND MOTIVATION

For the challenging problem of landmark tracking in X-ray locomotion scenarios, Active Appearance Model (AAM) (Cootes et al., 1998; Edwards et al., 1998; Cootes et al., 2001; Matthews and Baker, 2004) based approaches have successfully been applied in several variations in recent years (Haase et al., 2011; Haase and Denzler, 2013). One substantial practical drawback for the application to large amounts of recorded data, however, is that AAMs need to be trained on labeled example data (Haase and Denzler, 2011a). Furthermore, as for instance described in (Gross et al., 2005), trained AAMs do not generalize well to unseen cases. In our scenario, this includes changes in locomotion behavior or birds of different morphology. Therefore, AAMs are in general only applicable for the particular locomotion sequence they were trained on. Our goal in this paper is to overcome these practically relevant shortcomings for X-ray locomotor tracking by using a solely data-driven approach without any need of training data.

One possibility for entirely data-driven tracking are standard local approaches such as optical flow or template matching. In (Amthor et al., 2012), however, it is shown that not only these standard methods, but also an occlusion-robust extension of template matching fails to track all landmarks due to local ambiguities and disturbances. Based on these findings, the data-driven method to be employed must be global, *i.e.* the locomotor system must be modeled as a whole.

A prominent method which allows data-driven modeling of articulated objects is the concept of pictorial structures (Felzenszwalb and Huttenlocher, 2005; Felzenszwalb and Huttenlocher, 2000; Fischler and Elschlager, 1973), a form of deformable part-based models (Felzenszwalb et al., 2010). Depending on the type of appearance model, no training is necessary (Felzenszwalb and Huttenlocher, 2000), al-

though more complex variations exist which rely on training data (Andriluka et al., 2009; Zuffi et al., 2012; Pishchulin et al., 2013). Due to frequent self-occlusions of relevant anatomical parts during locomotion, however, standard pictorial structures without any form of occlusion handling are likely to fail in our X-ray scenario. Therefore, in this work we aim to extend global pictorial structure models (Felzenszwalb and Huttenlocher, 2000) with robust local matching approaches (Amthor et al., 2012) to combine the advantages of global modeling and local occlusion robustness while still avoiding the need of training data.

3 BACKGROUND

In the following, a brief overview of the two main approaches which form the base of our robust part-based skeleton tracking method are presented, namely *sub-template matching* and *pictorial structures*.

3.1 Sub-template Matching

The basic idea of standard template tracking is to extract a template \mathbf{T} in the first image of a sequence $\mathbf{I}_1, \dots, \mathbf{I}_L$ and to recover the best matching template configuration such as position (x, y) , orientation θ , or scale s in subsequent frames. This procedure is based on a particular matching function $f_{\mathbf{T}}(\mathbf{I}, (x, y, \theta, s))$ which determines how well template \mathbf{T} matches image \mathbf{I} given the template configuration (x, y, θ, s) . A typical choice for f is based on the *cross correlation coefficient*, which can efficiently be computed using the frequency domain. The optimal transformation $(\hat{x}, \hat{y}, \hat{\theta}, \hat{s})$ of a template \mathbf{T} with respect to an image \mathbf{I} is given by

$$(\hat{x}, \hat{y}, \hat{\theta}, \hat{s}) = \operatorname{argmax}_{x, y, \theta, s} f_{\mathbf{T}}(\mathbf{I}, (x, y, \theta, s)). \quad (1)$$

One major disadvantage of standard template matching is its failure in the case of occlusions (Amthor et al., 2012), as even partial disturbances in the search image \mathbf{I} can drastically bias the template matching results. The main idea of *sub-template matching* (Jurie and Dhome, 2002; Ishikawa et al., 2002) is to overcome this problem by exploiting the fact that non-occluded parts of an image can still be used to estimate the correct template transformation when considering them individually. As suggested in (Jurie and Dhome, 2002; Ishikawa et al., 2002) this approach can be implemented by dividing the entire template \mathbf{T} into K sub-templates $\mathbf{S}_1, \dots, \mathbf{S}_K$ and determining the score function for each of them independently. The main challenge then is to merge

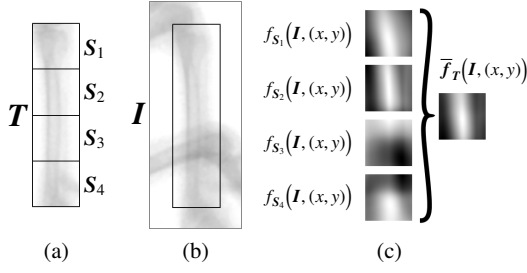


Figure 2: Sub-template matching example: (a) Original template T showing an X-ray recording of a bird's leg. The template is split into four sub-templates S_1, \dots, S_4 . (b) Search image I with partial occlusion. (c) Individual sub-template scores $f_{S_1}(I, (x, y)), \dots, f_{S_4}(I, (x, y))$ and averaged score $\bar{f}_T(I, (x, y))$. Rotation and scale were omitted in this example for the sake of clarity. The matching results for the non-occluded sub-templates S_1, S_2, S_4 are consistent, while S_3 provides erroneous estimates caused by occlusions. The final template score $\bar{f}_T(I, (x, y))$ in the right-most column, however, shows that the biased matching of S_3 is averaged out and a correct estimation for the entire template is obtained.

the matching results of all sub-templates into one final estimation for the entire template. In both (Jurie and Dhome, 2002) and (Ishikawa et al., 2002), this task is solved by making a hard decision for each sub-template, *i.e.* each sub-template votes for exactly one possible transformation. In contrast, (Amthor et al., 2012) use a soft approach for sub-template fusion which is motivated by three fundamental observations for occlusions in the given X-ray scenario: (i) non-occluded sub-templates provide correct matching results, (ii) partially occluded sub-templates might still provide a peak at the correct position in the pose space, and (iii) full occlusions of sub-templates provide random matching results. As a consequence, the fusion of all sub-templates is performed by averaging their particular scores $f_{S_1}(I, (x, y, \theta, s)), \dots, f_{S_K}(I, (x, y, \theta, s))$ in the pose space, *i.e.*

$$(\hat{x}, \hat{y}, \hat{\theta}, \hat{s}) = \underset{x, y, \theta, s}{\operatorname{argmax}} \bar{f}_T(I, (x, y, \theta, s)) \quad (2)$$

with

$$\bar{f}_T(I, (x, y, \theta, s)) = \frac{1}{K} \sum_{k=1}^K f_{S_k}(I, (x, y, \theta, s)). \quad (3)$$

An example of this soft sub-template matching procedure is shown in Fig. 2 for the case of the X-ray scenario at hand. In Fig. 2(a), the original template T including its division into sub-templates S_1, \dots, S_4 is depicted. Fig. 2(b) shows a scenario in which the original template is partially occluded by another anatomical structure. The resulting matching scores $f_{S_1}(I, (x, y)), \dots, f_{S_4}(I, (x, y))$ are shown in the left

column of Fig. 2(c), but only template translation (x, y) is considered for the sake of simplicity. It can be seen that the non-occluded sub-templates S_1, S_2, S_4 have correct matching results, while S_3 is occluded and does not match correctly. The final template score $\bar{f}_T(I, (x, y))$ is given in the right column of Fig. 2(c) and shows that the erroneous result of the occluded sub-template is averaged out.

3.2 Pictorial Structures

Pictorial Structures (PS) (Felzenszwalb and Huttenlocher, 2000; Felzenszwalb and Huttenlocher, 2005; Fischler and Elschlager, 1973) are an instance of deformable part-based models, *i.e.* an object is represented by connected rigid sub-components. In the case of pictorial structures, the parts are connected by spring-like connections, and the appearance of each part can be modeled in a general manner, allowing for intensity features as well as for more complex feature representations (Felzenszwalb and Huttenlocher, 2000). The connections between parts of a pictorial structures model are represented by a graph $G = (V, E)$, where the vertices $V = \{v_1, \dots, v_N\}$ correspond to the N model parts and the edges $E \subseteq V \times V$ specify pairwise connections between those parts. While in general the structure of G can be arbitrary, in the following we assume a tree structure as this allows for an efficient optimization of the model (Felzenszwalb and Huttenlocher, 2000).

Each instance of a given pictorial structures model is fully characterized by the configuration $I = (I_1, \dots, I_N)$, where I_n are the positional parameters such as position, orientation, and scale of part v_n . Given the part configuration I_n , the matching quality of part v_n with respect to an image I is denoted by $g_n(I, I_n)$. For the case of intensity features, $g_n(I, I_n)$ can easily be assessed via template matching. Additionally, for each pair (v_{n_1}, v_{n_2}) of connected parts, $h_{n_1, n_2}(I_{n_1}, I_{n_2})$ measures how likely the relative positioning of parts v_{n_1} and v_{n_2} is for a given model. The optimal configuration \hat{I} of a pictorial structures model for a search image I is then defined by

$$\hat{I} = \underset{I=(I_1, \dots, I_N)}{\operatorname{argmax}} \left(\sum_{v_n \in V} g_n(I, I_n) + \sum_{(v_{n_1}, v_{n_2}) \in E} h_{n_1, n_2}(I_{n_1}, I_{n_2}) \right). \quad (4)$$

As shown in (Felzenszwalb and Huttenlocher, 2000), the solution of this equation is equivalent to the maximum a posteriori (MAP) estimate and can efficiently be computed using dynamic programming.

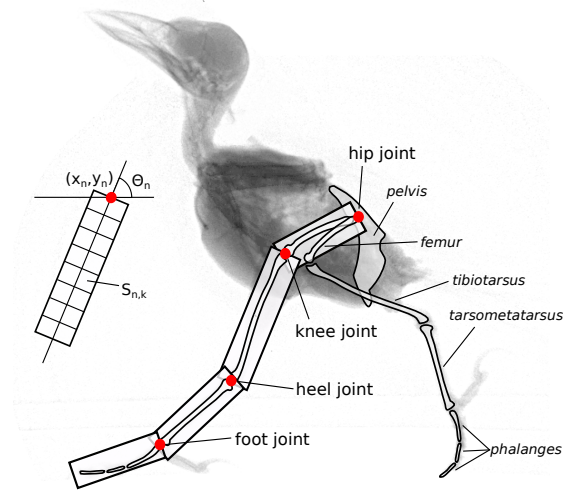


Figure 3: Schematic representation of the relationship between the anatomical structure of a bird (Nyakatura et al., 2012) and our part-based model approach (example showing one leg of a jackdaw). On the left hand, the division into sub-templates $S_{n,k}$ of a single part and the corresponding configuration I_n is shown.

4 ROBUST PICTORIAL STRUCTURES

In the following, our occlusion-robust extension of standard pictorial structures is presented in detail. While our approach is generic and can be applied to any kind of data standard pictorial structures are suited for, we focus on the X-ray animal skeleton tracking scenario as example application. Firstly, in Subsect. 4.1, we describe the extended pictorial structure framework. In Subsect. 4.2, optimization techniques for our extended model are presented.

4.1 Model Definition

Our basic model is identical to original pictorial structures (Felzenszwalb and Huttenlocher, 2000) as defined in Subsect. 3.2, *i.e.* the object to be tracked is divided into N parts whose connections are represented by a graph $G = (V, E)$. For a given model configuration I , the matching quality of a given pictorial structure can be assessed via Eq. 4. For our biological skeleton tracking application, the model has a tree structure originating at the pelvis, while the remaining parts cover the two legs, with a single bone per part. In this specific application, there is no need for spring-like connections between individual model parts used in (Felzenszwalb and Huttenlocher, 2000). Instead, we use revolute joints similar to anatomical

joints, which simplifies Eq. 4 to

$$\hat{I} = \operatorname{argmax}_{I=(I_1, \dots, I_N)} \sum_{v_n \in V} g_n(I, I_n). \quad (5)$$

Note, however, that this simplification is not essential for the extension presented in the following.

To include robust sub-template tracking into the pictorial structures model defined above, we choose the matching function g_n to be based on template matching as in (Felzenszwalb and Huttenlocher, 2000). This step allows us to easily replace g_n with the robust sub-template-based version \bar{f}_n (*cf.* Eq. 3), *i.e.* the matching quality of each part v_n with regard to a given image I is assessed on a sub-template basis. As a result, we can insert the sub-template matching formulation from Eq. 3 into Eq. 5 and obtain

$$\begin{aligned} \hat{I} &= \operatorname{argmax}_{I=(I_1, \dots, I_N)} \sum_{v_n \in V} \bar{f}_n(I, I_n) \\ &= \operatorname{argmax}_{I=(I_1, \dots, I_N)} \sum_{v_n \in V} \sum_{k=1}^{K_n} f_{S_{n,k}}(I, I_n), \end{aligned} \quad (6)$$

where K_n is the number of sub-templates of part v_n , $S_{n,k}$ is the k^{th} sub-template of v_n , and $f_{S_{n,k}}(I, I_n)$ determines how well this sub-template matches the search image I for a given configuration I_n of v_n . With this formulation, the optimal model parameters $\hat{I} = (\hat{I}_1, \dots, \hat{I}_N)$ are specified, for which the pictorial structure best matches the given image I while being robust to local occlusions of the individual model parts.

4.2 Optimal Model Fitting

To fit the extended pictorial structure model to a given image I , several methods can be applied. The naïve way of a direct search—*i.e.* testing all reasonable parameter combinations of the model—is not of practical use, as it has a complexity which is exponential in the number of model parts N .

In (Felzenszwalb and Huttenlocher, 2000) it was shown that the paradigm of dynamic programming (DP) can be used to solve the original pictorial structures formulation. In the following, we show that this property still holds for our robust extension by presenting an optimal DP algorithm for Eq. 6. Following (Cormen et al., 2001), the main steps of DP in our scenario are (i) the recursive definition of an optimal solution, and (ii) the construction of an optimal solution, both of which will be described below.

Recursive Definition. We assume that the part connection graph G has a tree structure with root node

$v_{n_{\text{root}}}$. To reformulate the optimal solution, we define the function $F_n(\mathbf{I}, (x, y))$ which for every possible position (x, y) of part v_n gives the best matching quality of the entire sub-model consisting of v_n and all of its children. As schematically shown in Fig. 3, each part v_n determines the starting position (x', y') for each of its child parts, and consequently the optimal parameters for the sub-model containing v_n and all of its children depend on the matching quality of v_n itself and the matching quality of all child parts of v_n . For any leaf node $v_{n_{\text{leaf}}}$, however, no child parts are present, and the optimal parameters only depend on the matching quality of $v_{n_{\text{leaf}}}$ and the starting point (x', y') defined by the parent part of $v_{n_{\text{leaf}}}$. Thus, the optimal solution for the full model can be formulated recursively in a bottom-up fashion by starting with all leave nodes $v_{n_{\text{leaf}}}$, for which we have

$$F_{n_{\text{leaf}}}(\mathbf{I}, (x, y)) = \max_{\theta, s} \bar{f}_{n_{\text{leaf}}}(\mathbf{I}, (x, y, \theta, s)). \quad (7)$$

The optimal matching results of non-leaf parts can then be defined recursively by

$$F_n(\mathbf{I}, (x, y)) = \max_{\theta, s} \left(\bar{f}_n(\mathbf{I}, (x, y, \theta, s)) + \sum_{v_m \in \text{ch}(v_n)} F_m(\mathbf{I}, (x', y')) \right), \quad (8)$$

where $\text{ch}(v_n)$ denotes the set of all child nodes of v_n and (x', y') is the starting position of all child nodes of v_n and is entirely determined by the configuration of v_n . To be able to recover the optimal values of θ and s in a later step, we additionally define the function $Q_n(\mathbf{I}, (x, y))$ as the argmax equivalent of Eq. 8, *i.e.*

$$Q_n(\mathbf{I}, (x, y)) = \arg\max_{\theta, s} \left(\bar{f}_n(\mathbf{I}, (x, y, \theta, s)) + \sum_{v_m \in \text{ch}(n)} F_m(\mathbf{I}, (x', y')) \right). \quad (9)$$

In terms of the recursive definition given in Eq. 8, the globally optimal matching score F_{global} for the entire model is given by

$$F_{\text{global}} = \max_{x, y} F_{n_{\text{root}}}(\mathbf{I}, (x, y)). \quad (10)$$

Note that for above scheme the *memoization* technique should be used to avoid redundant calculations by re-using previously computed values.

Construction of Optimal Solution. Due to the bottom-up recursive formulation of the optimization problem, the solution can now be constructed in a top-down manner starting with $v_{n_{\text{root}}}$. Based on Eq. 10, the

globally optimal position $(\hat{x}_{n_{\text{root}}}, \hat{y}_{n_{\text{root}}})$ of $v_{n_{\text{root}}}$ can be found via

$$(\hat{x}_{n_{\text{root}}}, \hat{y}_{n_{\text{root}}}) = \arg\max_{x, y} F_{n_{\text{root}}}(\mathbf{I}, (x, y)). \quad (11)$$

The remaining configuration parameters of $v_{n_{\text{root}}}$, *i.e.* $\hat{\theta}_{n_{\text{root}}}$ and $\hat{s}_{n_{\text{root}}}$ can then be obtained from $Q_{n_{\text{root}}}$ via

$$(\hat{\theta}_{n_{\text{root}}}, \hat{s}_{n_{\text{root}}}) = Q_{n_{\text{root}}}(\mathbf{I}, (\hat{x}_{n_{\text{root}}}, \hat{y}_{n_{\text{root}}}). \quad (12)$$

On the basis of $\mathbf{l}_{n_{\text{root}}} = (\hat{x}_{n_{\text{root}}}, \hat{y}_{n_{\text{root}}}, \hat{\theta}_{n_{\text{root}}}, \hat{s}_{n_{\text{root}}})$, the position $(\hat{x}_{n_{\text{ch}}}, \hat{y}_{n_{\text{ch}}})$ of each child node $v_{n_{\text{ch}}} \in \text{ch}(v_{n_{\text{root}}})$ of $v_{n_{\text{root}}}$ can be calculated. These values, in turn, can then be used to look up $\hat{\theta}_{n_{\text{ch}}}$ and $\hat{s}_{n_{\text{ch}}}$ for each child node using $Q_{n_{\text{ch}}}(\mathbf{I}, (\hat{x}_{n_{\text{ch}}}, \hat{y}_{n_{\text{ch}}}))$. The reconstructed optimal configuration $\mathbf{l}_{n_{\text{ch}}} = (\hat{x}_{n_{\text{ch}}}, \hat{y}_{n_{\text{ch}}}, \hat{\theta}_{n_{\text{ch}}}, \hat{s}_{n_{\text{ch}}})$ can now be used to determine the optimal starting point for the child nodes of $v_{n_{\text{ch}}}$ itself—this process is repeated until a leaf node is reached. Once all leaf nodes have been processed, the full globally optimal model configuration $\hat{\mathbf{l}} = (\hat{\mathbf{l}}_1, \dots, \hat{\mathbf{l}}_N)$ is determined.






5 EXPERIMENTS AND RESULTS

In the following, we present evaluations of our proposed method which are based on a wide variety of real-world X-ray bird locomotion datasets. We use a total of 24 individual locomotion sequences which comprise quails, a bantam chicken, jackdaws, tinamous, and lapwings. All sequences were recorded for zoological and biomechanical studies presented in (Stoessel and Fischer, 2012, quails, jackdaws, tinamous), (Nyakatura et al., 2012, lapwing), and (Haase and Denzler, 2011b, bantam, one quail). All datasets were acquired at a frame rate of 1000 frames per second and at a resolution of 1536×1024 pixels. Ground truth landmarks were provided by biological experts for at least every 10^{th} frame of a sequence. In total the data used for the evaluations contains more than 33,000 frames and 150,000 manual landmark annotations. An overview of the examined datasets is presented in Table 1.

Because the recorded X-ray images also contain non-animal objects (*i.e.* background) such as the treadmill, the background information was automatically removed from all images prior to the evaluation using the method suggested in (Haase et al., 2013). The qualitative evaluation is based on the Euclidean distance between the tracking results and the corresponding ground truth landmark positions.

We compared our method to original pictorial structures (Felzenszwalb and Huttenlocher, 2000) and to established methods for X-ray locomotion analysis, namely single bone sub-template matching (Amthor

Table 1: Overview of the 24 real-world bird locomotion datasets used for experimental evaluation. The datasets were recorded during the studies presented in (Stoessel and Fischer, 2012, quails, jackdaws, tinamous), (Nyakatura et al., 2012, lapwing), and (Haase and Denzler, 2011b, bantam, one quail).

	SPECIES					TOTAL
	QUAIL (<i>Coturnix coturnix</i>)	JACKDAW (<i>Corvus monedula</i>)	TINAMOU (<i>Eudromia elegans</i>)	BANTAM (<i>Gallus gallus</i>)	LAPWING (<i>Vanellus vanellus</i>)	5
EXAMPLE IMAGES						
INDIVIDUALS/ SEQUENCES	5/9	3/6	2/6	1/1	1/2	12/24
FRAMES	13,841	9,080	6,070	796	3,528	33,315
GROUND- TRUTH LANDMARKS	49,652	20,761	70,002	2,160	7,500	150,075

et al., 2012), standard AAMs (Haase and Denzler, 2011a), and augmented AAMs (Haase and Denzler, 2013). The underlying part model—used for standard pictorial structures as well as for our method—comprises 8 parts as shown in Fig. 5 and was constructed based on the anatomical structures *pelvis*, *femur*, *tibiotarsus*, and *tarsometatarsus*. The root is located at the *pelvis* and contains both legs as child parts. For each sequence, we initialize the part-model by using one manually annotated frame. Note that for the application at hand, this initial frame is chosen to feature as few occlusions as possible, but occlusions can not be avoided entirely. However, we apply no special treatment for the initialization process and let our algorithm handle the occlusions. In subsequent frames, the initial model configuration is predicted by a Kalman filter framework. The search space between two frames was set to 35×35 pixels for translation, $\pm 5^\circ$ for rotation and 2% for scale. For the other methods, the same parameter settings as suggested in the original papers were used. In addition to quantitative results (cf. Fig. 4), qualitative results are provided in Fig. 5.

5.1 Comparison to Standard Pictorial Structures

As mentioned in the previous sections, general template matching used for pictorial structures can not deal with severe occlusions occurring in the X-ray datasets. To verify this assertion, we tested standard pictorial structures (Felzenszwalb and Huttenlocher, 2000) and compared the results to our final approach. To ensure a fair comparison, both our method and pictorial structures use the identical framework and only differ in the template matching method.

Fig. 4 shows the quantitative tracking results for all 24 datasets by landmark groups. As can be seen,

tracking median errors can be reduced substantially by our approach for almost all landmark groups, especially for the knee landmarks. Here, the error of 20–25 pixels is decreased to 10–15 pixels. The improvement of tracking performance becomes even more distinct when considering the upper quartile errors. For standard pictorial structures, these errors range between 45 and 80 pixels for knee, heel, and foot joints. In contrast, our approach does not exceed the limit of 25 pixels for all landmarks. Hip landmarks, however, show slightly larger errors compared to the standard pictorial structures. Summing up, however, we can state that our presented approach is clearly more robust and achieves a higher accuracy than standard pictorial structures.

5.2 Comparison to Single Bone Tracking

The tracking framework presented in (Amthor et al., 2012) was designed to reliably determine the motion of outer torso landmarks via the tracking of single bones.

Again, the results for all available datasets are presented in Fig. 4. As can be seen, the performance of the single bone method in the case of the foot landmarks is slightly better than the performance of our approach. This can be explained by the fact that the single bone method was especially designed for tracking the *tarsometatarsi* and the heel and foot landmarks. Thus, it is to be expected that for these landmark groups the single bone technique is superior to the combined skeleton model tracker, as no further context has to be considered. In the case of the hip landmarks, the single bone approach provides better results on average. This behavior is a bit surprising at first, since severe ambiguities should disturb the tracking results without global knowledge about

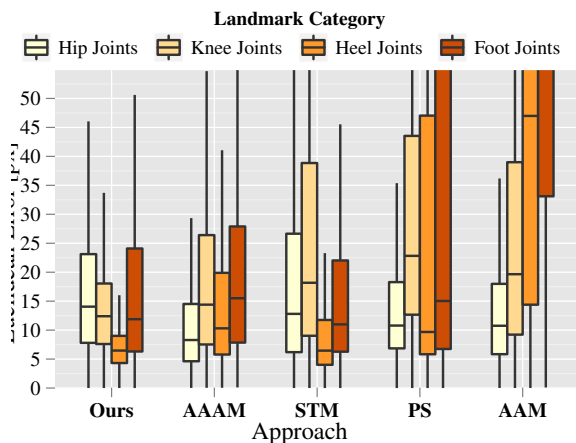


Figure 4: Quantitative evaluation of our approach compared to pictorial structures (PS) (Felzenszwalb and Huttenlocher, 2000), single bone sub-template matching (STM) (Amthor et al., 2012), standard active appearance models (AAM) (Haase and Denzler, 2011a), and augmented Active Appearance Models (AAAM) (Haase and Denzler, 2013). Our presented approach clearly outperforms PS and AAM and slightly improves established methods for X-ray locomotion while avoiding the need of training data.

the remaining anatomical structures. However, landmarks of both hips are very close to each other and confusions about the actual leg are unlikely to cause large tracking errors. Thus, substantial errors should occur for the single bone tracker at the knee landmarks if ambiguities are resolved incorrectly considering the *femur* or the *tibiotarsus* which can be confirmed considering Fig. 4. Here the median error is improved by 5 pixels while the upper quartile error is improved by even 20 pixels. This advantage of our approach is an important improvement of the single bone tracker, as an exact distinction of the knee landmarks is crucial for biological applications.

5.3 Comparison to AAMs

As discussed in Sect. 2, AAMs are well-studied for the given X-ray locomotion domain. To evaluate our approach, a comparison to standard AAMs (Haase and Denzler, 2011a; Haase et al., 2011) as well as a comparison to augmented AAMs (Haase and Denzler, 2013) is conducted on all 24 available datasets.

The tracking results for all 24 datasets are shown in Fig. 4. The worst results for outer-torso landmarks are obtained by standard AAMs, which is caused by non-linear shape activities and non-discriminative texture information of the lower leg landmarks. As augmented AAMs were designed to overcome these drawbacks of standard AAMs, results of the former are more consistent and have a median error of merely 10–15 pixels for all landmarks.

Our approach, however, provides worse results for the hip landmarks for reasons discussed in Subsect. 5.1. Errors for the lower leg landmarks, on the other hand, are slightly smaller. Considering the third quartile, our approach shows an improvement of 10 pixels for the knee and heel joints compared to augmented AAMs. Based on the fact that our method only has to be initialized for the first frame while AAMs require a substantial amount of annotated training images, we can state that our approach is more suited for the application to large amounts of data.

5.4 Runtimes

The presented combined skeleton model tracking framework was solely implemented in C/C++ using the OpenCV library v2.4. The experiments were performed on an Intel® Core™ 2 Duo CPU E8400 standard desktop computer @3.00 GHz. The tracking speed obtained in our experiments was about 0.5 frames per second on average. For one frame, the computation is performed for all landmarks of the entire locomotor system, *i.e.* hip, knee, heel, and foot landmarks of both legs. Similar to (Amthor et al., 2012), the computation times heavily depend on the number of used sub-patches. Hence, it is possible to decrease computational effort by reducing tracking reliability. In our scenario, accuracy is much more important than real time tracking—thus, the parameters were selected accordingly.

6 CONCLUSIONS AND FURTHER WORK

We have presented a robust, fully data-driven approach for the combined locomotor system tracking in X-ray videography of bird locomotion. By the fusion of robust single bone tracking and pictorial structure models, we are able to reliably track most of the landmarks even in cases of severe occlusions and consequential occurring ambiguities. The main benefit of our approach is the capability to only need one labeled frame to train the model, whereas model-driven approaches such as AAMs, deformable part models and sample based methods require a substantial amount of training samples. Furthermore, even unseen cases can be handled reliably, in contrast to existing model-driven methods. Based on exhaustive experiments we showed that our combined approach is comparable to established methods of the X-ray locomotion analysis scenario, while non-specialized methods were clearly outperformed.

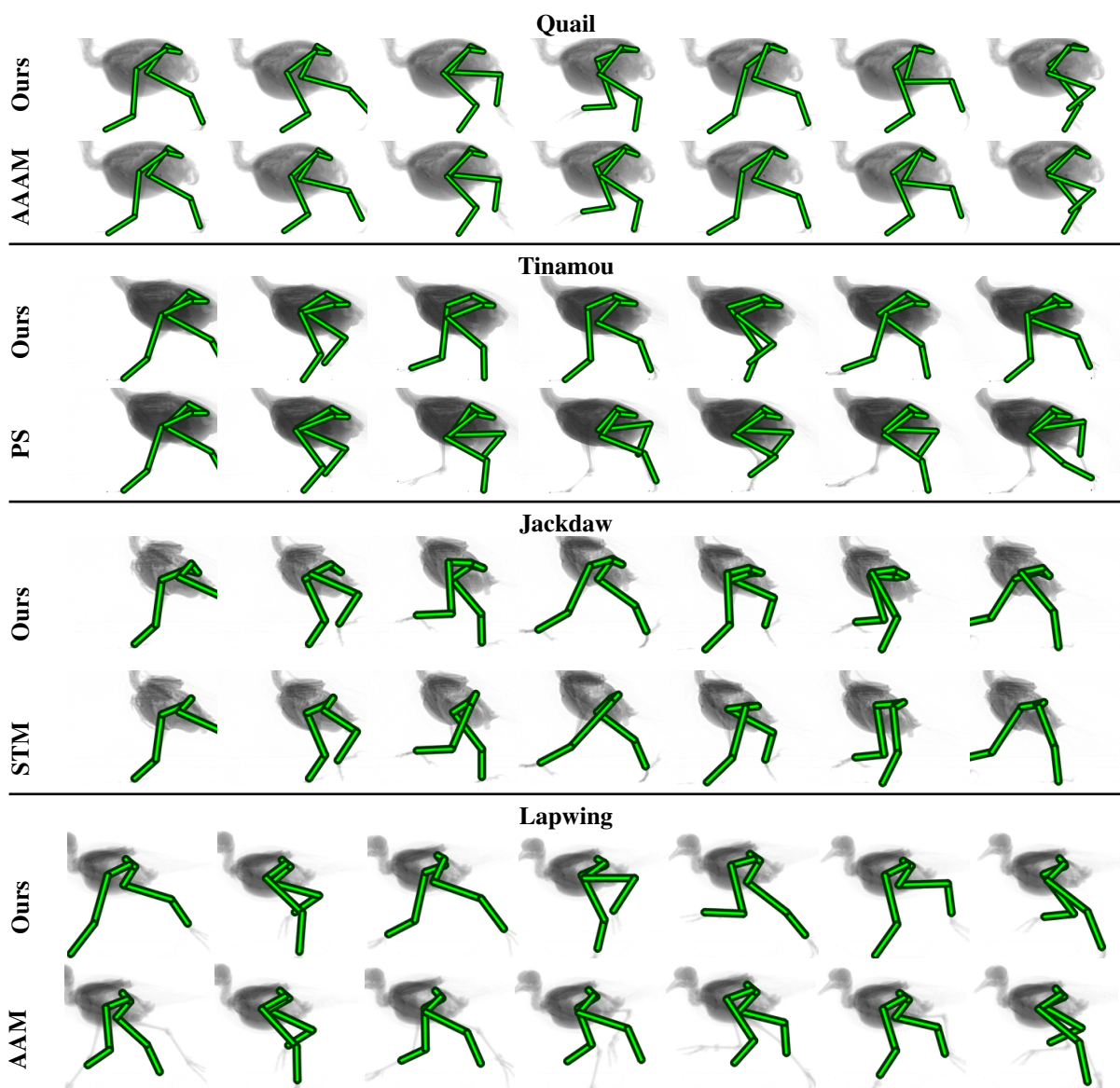


Figure 5: Qualitative evaluation of our approach compared to results obtained by pictorial structures (PS) (Felzenszwalb and Huttenlocher, 2000), single bone sub-template matching (STM) (Amthor et al., 2012), standard Active Appearance Models (AAM) (Haase and Denzler, 2011a), and augmented Active Appearance Models (AAAM) (Haase and Denzler, 2013).

An interesting point for future work would be the extension to a 3D model using further camera views, both X-ray as well as visible light cameras.

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