

Facial Paresis Index Prediction by Exploiting Active Appearance Models for Compact Discriminative Features

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Abstract: In the field of otorhinolaryngology, the dysfunction of the facial nerve is a common disease which results in a paresis of usually one half of the patients face. The grade of paralysis is measured by physicians with rating scales, e.g. the Stennert Index or the House-Brackmann scale. In this work, we propose a method to analyse and predict the severity of facial paresis on the basis of single images. We combine feature extraction methods based on a generative approach (Active Appearance Models) with a fast non-linear classifier (Random Decision Forests) in order to predict the patients grade of facial paresis. In our proposed framework, we make use of highly discriminative features based on the fitting parameters of the Active Appearance Model, Action Units and Landmark distances. We show in our experiments that it is possible to correctly predict the grade of facial paresis in many cases, although the visual appearance is strongly varying. The presented method creates new opportunities to objectively document the patients progress in therapy.

1 INTRODUCTION

Facial paresis is an often occurring disease and caused by a dysfunction of the facial nerve (Nervus facialis). Typical symptoms are a complete or partial loss of control for one side of the face with visible asymmetries between the hemispheres. Facial paresis can occur in every age (Alberti and Biagioni, 1972; Peitersen, 2002) and regardless of gender (Peitersen, 2002).

The causes of facial paresis are manifold and range from brain damage in certain areas over virus infections (Lyme disease) to muscle weakness (Myasthenia gravis) (Peitersen, 2002). However, in some cases no direct cause can be determined as in the case of Bell's palsy. All causes of the illness have in common that patients are not able to move one side of their face and possibly suffer from both their disease and a decreased life quality, e.g. problems with eating and drinking or to be unable to close one eye completely (Guntinas-Lichius et al., 2007).

The intensity of a facial paresis can be measured in different ways, as for example by rating the ability to control one specific muscle of the face (Stennert et al., 1977) or by judging the ability of facial movement during exercises (House and Brackmann, 1985). Both are determined by visual assessment and there-

fore rely on the clinical experience of the rating physician. With the help of these indices the actual degree of paralysis will be measured and therefore also a possible progress of recovery, as presented in this work.

The automated recognition of those indices will assist physicians to rate and compare patients facial paresis severity and identify potential recovery immediately. For analysis, additional equipment is not needed. Therefore it is possible to rate patients paresis index from a distance, potentially at home.

The House-Brackmann index is the most common grading system for facial paresis, developed in 1985 by (House and Brackmann, 1985). It consists of six grades, where a normal face is rated with grade I and a completely paralysed half of the face with no movement at all is rated with grade VI. The detailed description for every grade can be seen in Table 1.

In contrast to the House-Brackmann-Grading scale, the Stennert index does not rate the quality of facial movement as a whole. It is divided into the Stennert Index in Motion (SIM) and the Stennert Index at Rest (SIR). The SIR is determined on the patient completely relaxed face. However, for the grading of the SIM the patient has to perform exercises were each exercise activates only one facial muscle or group of muscles (nose wrinkling, eye closure, lip puckering, etc.). For every patient a physician has to

Table 1: House-Brackmann Grading System for facial palsy (House and Brackmann, 1985).

Grade	Dysfunction	Characteristics
I	Normal	Normal function in all areas
II	Mild	Gross: Slight weakness noticeable on close inspection; may have very slight synkinesis At rest: normal symmetry and tone Motion: Forehead: moderate to good function Eye: complete closure with minimum effort Mouth: slight asymmetry
III	Moderate Dysfunction	Gross: obvious but not disfiguring difference between two sides; noticeable but not severe synkinesis, contracture, and/or hemifacial spasm At rest: normal symmetry and tone Motion: Forehead: slight to moderate movement Eye: complete closure with effort Mouth: slightly weak with maximum effort
IV	Moderately severe Dysfunction	Gross: obvious weakness and/or disfiguring asymmetry At rest: normal symmetry and tone Motion: Forehead: none Eye: incomplete closure Mouth: asymmetric with maximum effort
V	Severe Dysfunction	Gross: barely perceptible motion At rest: asymmetry Motion: Forehead: none Eye: incomplete closure Mouth: slight movement
VI	Total paralysis	No movement

Table 2: Grading System for facial palsy (Stennert et al., 1977).

	Questions
SIR	Difference between lid fissure larger than 3mm?
	Existing ectropion?
	Nasolabial groove not visible?
	Height difference between mouth corners more than 3mm?
SIM	Frowning possible (raise eyebrow more than 50%)?
	Visible fissure in sleeping position (eyes closed)?
	Visible fissure while squinting?
	Canine teeth (top and bottom) not visible when showing teeth?
	Upper second incisor not visible when showing teeth (full width)?
	Difference of distance between philtrum and mouth corner more than 50% compared to healthy side while pursing lips?

answer the corresponding questions (see Table 2) with yes or no. The sum of answers form the final SIM.

The actual available tools and works either need physical markers on the patients face, used a very small patients dataset or did not use a common grading system. Some methods use physical markers in the face that were automatically detected and used for distance calculation and comparison (Wachtman

et al., 2001). Thus it is a non-invasive technique, it is not irritation free as markers have to be painted on the patients face. Only to detect the presence of a facial palsy automatically is not sufficient as the grade of the disease is also important to measure the progress of therapy (Gebhard et al., 2000). To rate a patients grade of palsy, the definition of new rating systems based on pre-calculated facial features seems feasible (Wang and Qi, 2005). Unfortunately those kind of indices were not accepted by physicians. This problem can be solved by using common rating systems like the House-Brackmann scale. Since the difference between grade II-III and IV-V is small, it is possible to use a reduced House-Brackmann index with only four degrees of palsy (Gebhard et al., 2001). With the use of local binary patterns or the Hamming distance between the left and the right side of the face and a classification method the entire HB index can be predicted (He et al., 2009; Song et al., 2013).

We present a novel and fast non-invasive and irritation-free method for the automated prediction of grades for single-sided facial palsy patients using Random Decision Forests (Breiman, 2001) as described in Section 3. Since the method only uses images for prediction, there is no need for the patient being present during the analysis.

In Section 2, we give an overview about related work. The used methods which are the base of our approach and the proposed framework are presented in Section 3. In Section 4, we evaluate our framework

on real-world datasets and discuss the results.

2 RELATED WORK

A method to quantify facial motion was proposed by (Wachtman et al., 2001). Based on physical markers in the subjects face they tracked the movement of these markers and calculated the distances between them over time. The results were plotted and shown to experts for further use. Their approach was not a fully automated grading system but supposed to assist physicians in the clinic or the doctor's office.

(Gebhard et al., 2000) published an image-based system to detect single-sided facial paresis without the usage of physical markers. They extracted the person in the image via segmentation and calculated asymmetries between the left and the right hemisphere. With this information, they were able to distinguish between healthy persons or patient diagnosed with facial paresis.

To detect not only patients with facial paresis but also the grades of facial paralysis, (Gebhard et al., 2001) used image sequences of patients performing exercises. They calculated the difference image and the optical flow between the healthy and the sick hemisphere of patients. With these features they trained a classifier to predict four grades of facial paresis. These grades based on the House-Brackmann index, however were condensed to four possible grades.

(He et al., 2009) presented an automated discriminative grading system for facial paresis patients based on the House-Brackmann-Score by using SVMs trained on Local Binary Patterns (LBP). They tested and trained their method on a video dataset and achieved good results. Unfortunately their dataset is not publicly available, thus comparison is not possible.

A more global method was developed by (Delanoy and Ward, 2010). They proposed an approach based on Active Appearance Models (AAM). After fitting the AAM to the target image they calculated the distances between the points with respect to the hemisphere and used these information to predict a facial paresis score. Although they did not test their method on real patients data they generally showed AAMs can be used to predict the House-Brackmann index.

A prediction method for the House-Brackmann score based only on a few single images was developed (Song et al., 2013). After detecting the edges of a patients image they calculated the Hamming distance for facial symmetry. The indices were pre-

dicted by an SVM combined with an Emergent Self-Organising Map. Unfortunately their training and test dataset only contained 46 patient data and 21 images of healthy persons. As in (He et al., 2009) the used dataset is not publicly available, hence direct comparison is not possible.

The work of (Haase et al., 2013) used AAMs on facial paresis patient images. Based on a Gaussian Process regression using the AAMs fitting-parameters the Action Units (AU) of the respective facial side were predicted.

In this work, we present a novel approach to predict the severity of a patients facial paresis. The detailed methods are described in the next section.

3 METHODS

To start the analysis of facial paresis patient images, a proper description method is needed. For the representation of faces, generative statistical models like Active Appearance Models (AAM) have demonstrated to be a powerful technique with applications in different areas (Cootes et al., 2001; Haase et al., 2014; Song et al., 2014; Vincent et al., 2010). Although there are more up-to-date methods for facial landmark detection to benefit from the AAMs representation of both shape and texture and use the extracted appearance parameters as features for classification of new and unseen images.

3.1 Framework

The proposed framework consists of three stages as seen in Figure 1: Initially the half sided AAM is trained on images of healthy persons with both neutral expressions and healthy people performing the exercises as can be seen in Figure 3. This trained AAM is then fitted on the patients images using multivariate linear regression (Matthews and Baker, 2004).

Depending on the used features for training the obtained features from the model fitting have to be pre-processed. Either the fitting parameters were used to predict AUs based on a pre-trained Gaussian Process regression (Haase et al., 2013) or the absolute distance between the left and the right side of the face or the Euclidean distance between the corresponding landmarks of each side. These information combined with the labeled facial paresis indices (Stennert or House-Brackmann index) were now used to train the classifier.

In our approach, a Random Decision Forest (RDF) was used to classify facial paresis indices (Breiman, 2001). For classification, also a k-Nearest-Neighbour

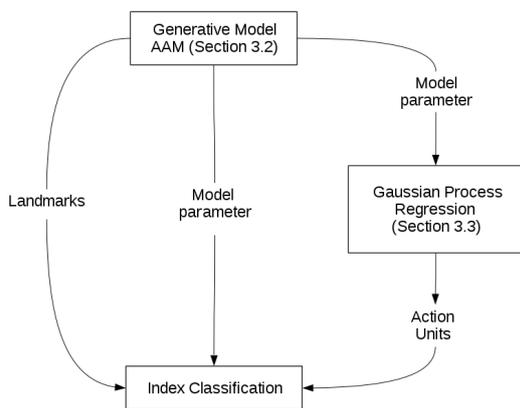


Figure 1: Overview of the framework for facial palsy index prediction.

approach and an SVM was tested for index prediction but we obtained much better results by using an RDF. The optimal parameters for the respective features were obtained via a parameter analysis. More detailed information and results can be found in Section 4.

3.2 Active Appearance Models

Based on a number of annotated images I_1, \dots, I_n showing instances of a specific object category, like faces, AAMs can be automatically trained. The resulting parametrised model can be fitted to new, yet unknown images. The model training consists of three parts: the shape model, the texture model and the appearance model. The shape model is trained on the landmarks of every image. For this reason, the vectorised shapes s_1, \dots, s_n are aligned according to their scale, rotation and translation. In combination they form the matrix $S = (s_1 - s_\mu, \dots, s_n - s_\mu)$ where s_μ denotes the mean shape. By applying Principle Component Analysis (PCA) on the matrix S , we obtain the shape eigenvectors P_S . Each shape s' can be represented by its shape parameters p'_s :

$$s' = s_\mu + P_S \cdot p'_s \text{ with } p'_s = P_S^T (s' - s_\mu) \quad (1)$$

In order to train the texture model, the vectorised and shape-normalised object textures t_1, \dots, t_n are needed. Similar to the shape model, PCA is performed to achieve the texture eigenvectors P_t . The texture parameters p'_t are defined like the shape parameters in Equation 1. In the last step the above defined models are combined to train the appearance model. Again PCA is applied on the combined and variance-weighted texture and shape models to obtain the appearance eigenvectors P_A . The appearance parameters p'_a can be calculated based on the eigenvectors P_A and

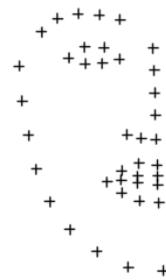


Figure 2: Shape of a half side AAM.

the shape as well as texture information of an object:

$$a' = P_A \cdot p'_a \text{ with } p'_a = P_A^T \cdot a' \quad (2)$$

Finally, a thus trained AAM can be fitted on new images via minimisation of the texture difference between the image and the model (Matthews and Baker, 2004).

Unfortunately, an AAM is generally trained on the entire face. This is not sufficient in the case of facial palsy patients images thus the model will not be able to deal with the asymmetries. The solution of this problem is to use an AAM trained only on one hemisphere of a face as done by (Haase et al., 2013; Delanoy and Ward, 2010). To obtain as much information as possible, the training dataset should contain images with the exercises the patients have to perform. An half side AAM represented by its shape-forming landmarks is shown in Figure 2.

Based on the assumption that we have a paralysed and a healthy side of a face, both hemispheres can be directly compared to each other by analysing the sides independently (Song et al., 2013; Haase et al., 2013).

3.3 Facial Feature Extraction

We used three different kinds of features, all based on the half-sided AAM fitted on the patients image.

First, we used the combined AAM-fitting-parameters for training. These parameters were used in three different ways: primarily, all available parameters were used, ordered by side (right, left) and the respective exercise the patients had to perform. We also calculated the absolute distance of both parameter vectors to obtain the difference between both hemispheres. By taking the absolute distance of the parameters, we ensure an independence from the respective paralysed side. Finally, we used only the parameters of the paralysed hemisphere without the healthy side.

As a second feature type, we used the resulting Action Units (AU) and their intensities from the approach of (Haase et al., 2013) for each half of the face.

Action Units (AU) are part of the Facial Action Coding System (FACS) used to parametrise human facial movement (Ekman and Friesen, 1978). Every muscle in the face is related to an AU and its activation level is coded on a scale from A (minimal activation) to E (maximal activation). The AU-prediction is based on a Gaussian Process regression using the fitting parameters of the half sided AAM to predict the activated AUs of a given face. This approach was evaluated on three different and widely used datasets with both images and labeled AUs. This model was then used to predict patients AUs in order to measure the muscle activity in both hemispheres. For our experiments we used a pre-trained model for AU prediction because neither landmarks nor AUs are available for our patient dataset.

As aforementioned for the AAM parameters we used three versions for training: all AUs with first the right and second the left half of the face, the Action Units of just the paralysed side and the absolute distance between the healthy and the paralysed side.

Finally, we took the fitted landmarks into account. Due to differences in position and size of the patients head during the image recording, the original landmarks can not be used. Therefore we calculated the Euclidean distance between the landmarks and their neighbours in order to describe the movement of these landmarks. If the paralysed half of the face is not able to do the exercises correctly the distances between the landmarks should be larger compared to the distances between two healthy hemispheres.

The extracted features were then used to train a Random Decision Forest.

4 EXPERIMENTS AND RESULTS

In the following we present the evaluation of our proposed method based on a dataset with real facial paresis patients data.

4.1 Dataset

The used dataset of patients with chronic facial paresis was provided by the universities ENT department. It contains images and information about 235 different patients of all ages with half sided facial paresis in different degrees of severity.

The information on every patient in the list were obtained by the physician on duty during their first visit in the hospital. These information contain the specification of the paralysed side (left or right hemisphere), the paresis form (partial or complete) and the

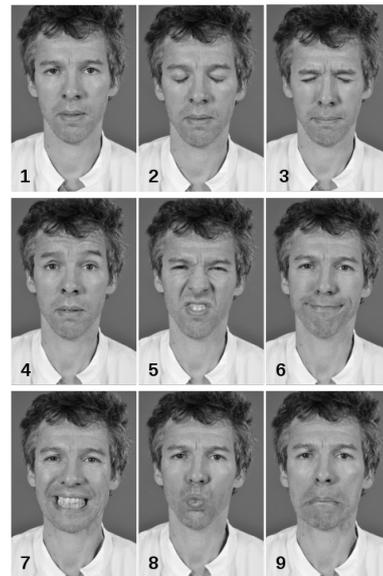


Figure 3: A healthy proband performing all nine exercises: resting face (1), closed eyes (2), squinting eyes (3), wrinkled forehead (4), wrinkled nose (5), smile with closed mouth (6), show teeth (7), pursing lips (8) and lowered mouth corners (9) (Haase et al., 2015).

grade of severity rated according to the Stennert index and House-Brackmann scale.

The images were taken soon after the first visit in the hospital. During the image recording the patients had to perform nine different exercises. These exercise images include a face in rest and several expressions that need different muscles to be activated as can be seen in Figure 3.

4.2 Index prediction

The overall prediction rates of all indices and methods can be seen in Table 6. These results were obtained by performing a 5-fold cross-validation and a parameter analysis to find the best combination of parameters for an optimal classification. To calculate the prediction rate we counted all prediction that differed by less than two grades from the ground-truth label as suggested by (He et al., 2009). This procedure is also motivated by the inter-rater variability observed by (de Ru et al., 2006; Coulson et al., 2005).

The results for each index to be predicted are discussed in detail in the next section.

Stennert Index in Rest

The Stennert Index in Rest (SIR) contains five different grades ranging from normal (0) to severe (4). More detailed information can be seen in Table 2. The analysis is performed on the image with the face in rest.

Table 3: Distribution of all Stennert Indices in Rest that were used for prediction during the crossvalidation (predictions in row and ground-truth in columns) and the distribution of indices in the used dataset.

	0	1	2	3	4
0	1	1	0	0	0
1	1	21	16	10	4
2	17	23	30	18	16
3	11	6	16	3	4
4	0	1	1	1	1
Dist:	37	52	63	32	25

Table 4: Distribution of all Stennert Indices in Motion that were used for prediction during the crossvalidation (predictions in row and ground-truth in columns) and the distribution of indices in the used dataset.

	0	1	2	3	4	5	6
0	0	0	0	0	0	0	0
1	0	0	1	0	0	2	2
2	1	0	1	2	1	2	5
3	0	0	0	2	4	2	9
4	2	3	6	6	9	10	21
5	0	6	5	8	18	8	23
6	1	4	2	0	4	3	4
Dist:	4	13	15	21	36	27	64

For training and testing there were a total 209 different patients data available. As can be seen in Table 3 the ground-truth data cluster in the middle. This also reflects the distribution of indices throughout the dataset (last row of Table 3). The majority of patients has a slightly visible paresis during rest. This can be a reason for the low recognition rate using this global approach: the index is obtained by scoring several regions in the face where the sum affirmed answers form the score.

The best results for the SIR were achieved by using the Action Units of the paralysed hemisphere or the distances between the landmarks provided by the AAM (c.f. Table 6) with the worst recognition rate 2.3 percentage points apart. Thus all three used feature versions seem to have nearly the same performance when predicting the SIR.

Stennert Index in Motion

Different to the Stennert Index in Rest the Stennert Index in Motion (SIM) is not based on one single image but on six different ones. Each image shows a different muscle movement (Figure 3) which has to be rated according to the rating scheme (Table 2).

To evaluate this index 180 different samples were used for training and testing. The ground-truth indices cluster in the right corner of Table 4. Similar

Table 5: Distribution of all House-Brackmann Indices that were used for prediction during the crossvalidation (predictions in row and ground-truth in columns).

	I	II	III	IV	V	VI
I	0	0	0	0	0	0
II	0	0	2	2	0	0
III	3	18	33	27	20	3
IV	0	21	17	15	3	0
V	0	0	1	0	0	0
VI	0	0	0	0	0	0
Dist:	3	39	53	44	23	3

to the SIR the SIM is calculated by summing up the answers of the questions to every image or muscle movement (Table 2). Hence, two patients can be rated with the same score but have totally different muscular defects.

Different to the SIR the used features differ in their recognition rate (Table 6). In general the AAM-fitting parameter provide the best recognition rate, especially the feature type that used all fitting parameters plus a variable that codes for the paralysed hemisphere (66.6%).

House-Brackmann Index

In contrast to the above discussed indices the House-Brackmann index (HB) does not rate single but all nine available images. The patients were observed during they perform the exercises and then rated according to the scheme (c.f. Table 1). According to (de Ru et al., 2006; Coulson et al., 2005) the variability through different experts is substantial.

To train and predict the HB index 165 dates from different patients were used. Like in the case of the SIR the predicted indices are grouped in the middle of the table.

This time both the fitting parameters and the Euclidean difference between the landmarks performed best with a recognition rate of 80.5% as can be seen in Table 6. The other fitting parameters were just by 0.5 percentage points worse than the best prediction rate. That indicates that the fitting parameters in general are suitable for the prediction of HB indices.

Throughout all indices the House-Brackmann index (HB) achieved the best recognition rates as can be seen in Table 6. As the manually obtained indices do not depend on single frames and local differences but on the general degree of paresis the global method performs best on the global index as expected.

Not focused on individual results of the different used features the AAM-fitting parameters performed best throughout the experiments especially in case of the Stennert Index in Motion. The recognition rates are also quite similar or differ just slightly by a few

Table 6: Prediction rate of the different features and indices. The used side variable defines the paresis side of the patient. A prediction was marked as true if the distance between predicted and measured index less or equal to one as suggested by (He et al., 2009).

Feature Types	Features	SIR	SIM	HB
AAM-fitting parameters	all parameters without side variable	70.0%	64.4%	80.0%
	all parameters with side variable	70.9%	66.6%	80.0%
	parameters of paralysed hemisphere	70.0%	65.5%	80.0%
	left-right absolute distance	70.0%	63.3%	80.5%
Action Units	all AUs without side variable	71.9%	57.2%	76.9%
	all AUs with side variable	71.9%	51.1%	76.3%
	AUs of paralysed hemisphere	72.3%	56.6%	74.5%
	left-right absolute distance	70.0%	58.2%	78.7%
Landmark distances	without side variable	71.4%	57.7%	80.5%
	with side variable	72.3%	57.7%	80.5%
	difference between sides	71.9%	57.2%	73.3%

percentage points. This strongly indicates that AAM-fitting parameters can be used in classification of facial paresis indices.

Comparison to Further Work

The approach by (He et al., 2009) achieved an overall recognition rate of 94.1% for the House-Brackmann index prediction. For this reason their prediction rates outperform our approach. Nevertheless these rates are not directly comparable as (He et al., 2009) used video sequences for their automated prediction and not single images.

The approach by (Delannoy and Ward, 2010) used Active Appearance Models for prediction and achieved an average recognition rate of 87% on their dataset. Again, these rates are not directly comparable. (Delannoy and Ward, 2010) did not test their approach on real patients data but on synthesised images that do not reflect the large variety of real patients images.

Unfortunately, there are no similar works that automatically predict the Stennert index, thus comparison is not possible.

4.3 Implementation Details

The presented framework was both implemented in R and C/C++. The fitting of the AAM on the patients images was done by an R framework. The index prediction was implemented in C/C++ using the OpenCV library version 2.4.10 (Bradski, 2000). The experiments were performed on a standard desktop computer (i5 760 CPU, 2.80 GHz). Fitting an AAM on one single image took about five Milliseconds. The prediction of the appropriate index less than one millisecond, hence one image is approximately classified within 5 milliseconds. This allows the analysis of large-scaled databases within a feasible amount of

time.

5 CONCLUSION

In this work the severity of a patients facial paresis is predicted automatically by using AAMs and an RDF. The standard procedure to obtain the severity of a facial paresis is to rate the index manually in the clinic by a physician. Possible rating schemes for facial paresis are the Stennert index and the House-Brackmann scale. The indices allow a documentation of the actual severity and the status of recovery during and after therapy. We propose an automatic method to rate a patients facial palsy based only on nine images. The method is irritation-free and objective. Also no interaction between patients and therapist is needed for prediction. First a pre-trained Active Appearance Model is fitted on only the images. Afterwards we used both the resulting fitting parameters, the distances between the fitted landmarks and the predicted Action Units (Haase et al., 2013) respectively to train a Random Decision Forest for classification. Especially for the House-Brackmann index we obtained a prediction rate of 80%.

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